

Segmentation of Synovitis

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Goals

- The volume of the inflamed synovia might be an early predictor for the severity of the disease (it is in the case of Osteoarthritis and Rheumatoid arthritis).
- Manual annotation of the inflamed synovia is extremely time-consuming and prone to variability.



Goal

provide a semi-automatic quantification method to **speed up** the process and **reduce variability**.

- T1W-FFE3D FAT, coronal MRI of wrists/hips, acquired at 1.5 min after injection of a contrast bolus.
- The contrast enhances the inflamed synovia, which can be segmented.
- Other structures are enhanced (blood vessels, sinew).



Approach: Segmentation as Classification

the segmentation problem is seen as a problem of classifying voxels

- manually annotated exams are used for training-validating-testing a set of classifiers, combined by bagging;
- the features are the intensities of the voxels and of their 1-neighbors (in 3D);
- each classifier is a linear combination of Gaussian kernels centered on the examples;
- the width of the kernels is chosen as the median distance between training examples;
- the training is performed by ν -method, an iterative method originally devised for solving inverse problems.

we need annotations for the whole training-validation-testing pipeline

- We provide a software tool for performing annotations.
- Freehand drawing was preferred to polylines.
- Current status:
 - 4 wrists by two clinicians (8 annotations)
 - 1 wrist annotated together



Features:

- loading and visualization of DICOM data;
- support for drawing, saving and loading freehand and elliptic annotations;
- works on different platforms: Win, Mac and Linux;
- controls on image zoom and contrast;
- misc: multiplanar view, maximum intensity projections, thresholding, ...

Analysis of Manual Annotations

Inter-observer analysis

- Correlation, per slice: $r = 0.92$, $p < 0.001$
- Absolute difference per slice, avg = 30.5%, median = 14.4%
- Absolute difference per exam, avg = 15.2%, median = 12.1%
- Classification overlap = 63.0%

Computed over 4 exams, with 2 different annotations

Sensitivity to Morphological Operations

- 1px Dilation (avg), per exam: 33.3%
- 1px Erosion (avg), per exam: -31.4%

Computed over 9 annotations.

Analysis of Training Examples

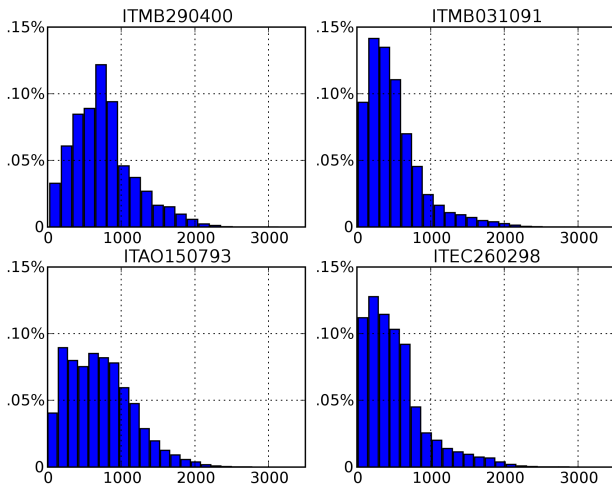
Percentage of overlap between histograms of the intensities for positive and negative examples.

The lower the overlap, the easier the classification task.

	Obs. 1	Obs. 2
ITAO	46.9%	55.3%
ITEC	29.5%	38.3%
ITMB03	35.9%	39.0%
ITMB29	35.8%	43.1%

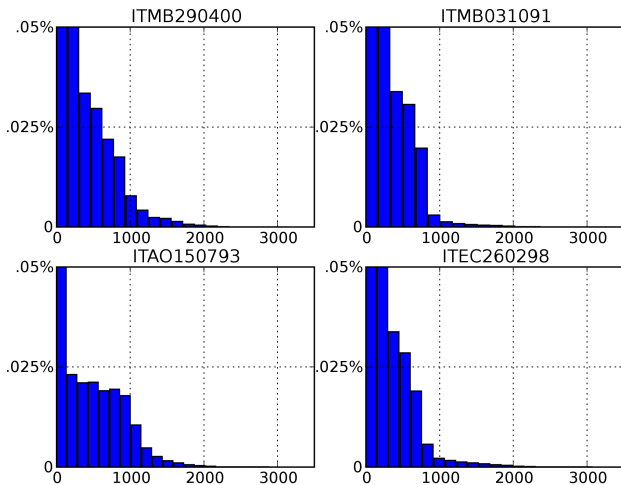
Analysis of Training Examples

Intensity histograms of the exemplar voxels (pos+neg).



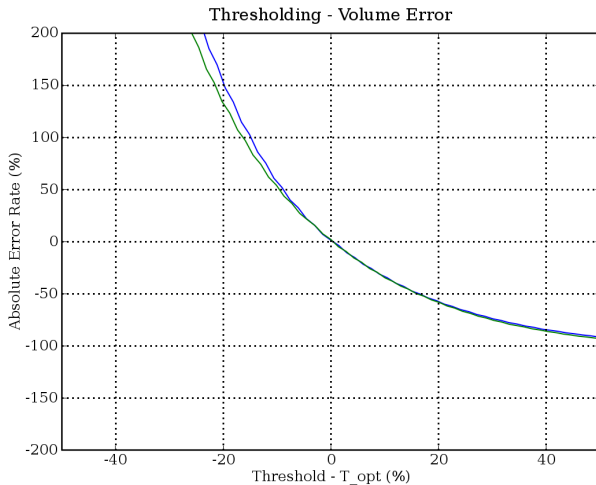
Analysis of Training Examples

Intensity histograms of all voxels.



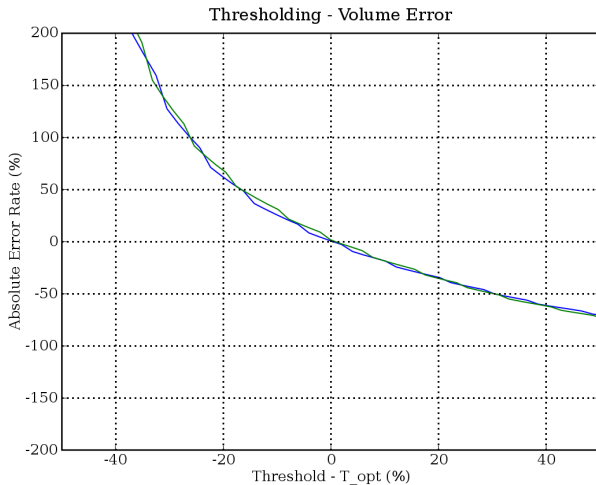
Analysis of Hard Thresholding

ITAO



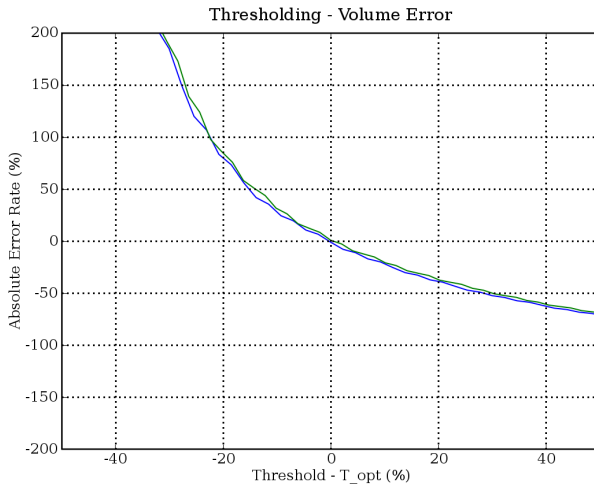
Analysis of Hard Thresholding

ITEC



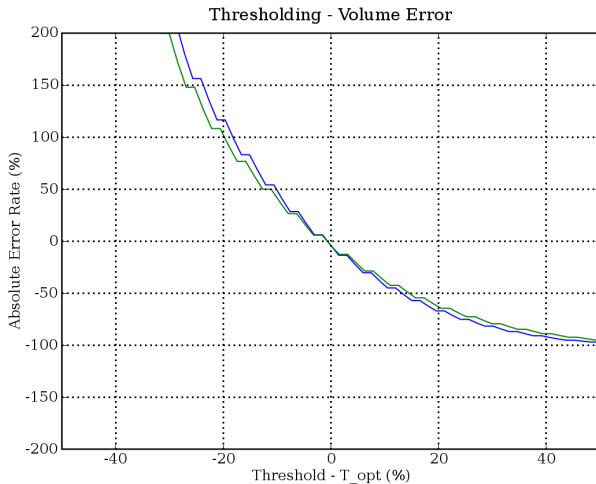
Analysis of Hard Thresholding

ITMB03



Analysis of Hard Thresholding

ITMB29



Experimental Setup

for each exam

- use the other exams for training and validation;
- train 5 classifiers on 1.000 voxels;
- validate each classifier on 5 different samples of 1.000 voxels;
- combine the classifiers by bagging (averaging);
- test the classifiers on 20.000 voxels;

the exemplar voxels are drawn from the annotated synovia (red contour) and surrounding regions (green contour).



Normalization by Ranking

examples from different exams have different intensity histograms

- one exam is randomly chosen as reference;
- the intensities of its voxels are sorted in an ordered list $I_r = (i_0, \dots, i_N)$, where N is the number of voxels and $i_j \leq i_{j+1}$ for $j = 0, \dots, N$;
- given another exam, the intensity of each voxel is set to the intensity of its equal-rank voxel in the reference exam; that is, if a voxel has rank k in the sorted list of intensities, then its new intensity will be i_k

Results

Results for classifiers trained and tested on one observer. **Normalized by ranking.** Tuning of the offset.

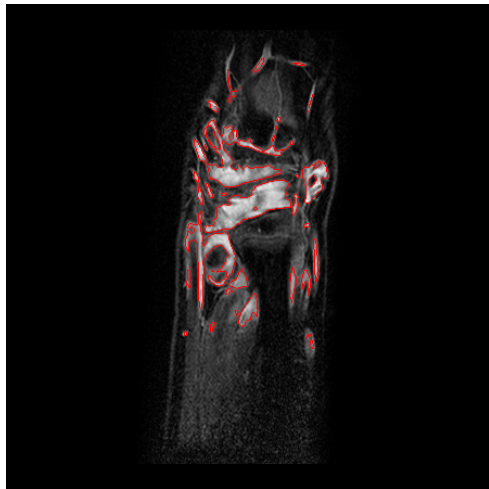
	b_0	$b_0 + 0.1$	$b_0 + 0.2$	$b_0 + 0.3$	$b_0 + 0.4$
	Classification Error				
ITAO	8.7%	8.9%	9.1%	9.6%	10.4%
ITEC	8.2%	7.8%	7.6%	7.4%	7.6%
ITMB03	7.7%	7.3%	7.6%	8.0%	8.4%
ITMB29	8.7%	8.9%	8.8%	9.4%	9.6%
mean	8.3%	8.2%	8.3%	8.6%	9.0%
σ	0.48%	0.81%	0.79%	1.07%	1.24%
	Volume Error				
ITAO	-38.4%	-21.1%	-12.3%	6.4%	22.6%
ITEC	-49.3%	-42.7%	-36.0%	-24.8%	-11.3%
ITMB03	-27.8%	-16.2%	-2.1%	11.2%	26.4%
ITMB29	-34.8%	-20.8%	-6.5%	5.1%	25.1%
mean	-37.6%	-25.2%	-14.2%	-0.5%	15.7%
σ	9.0%	11.9%	15.1%	16.4%	18.1%

Normalization Comparisons

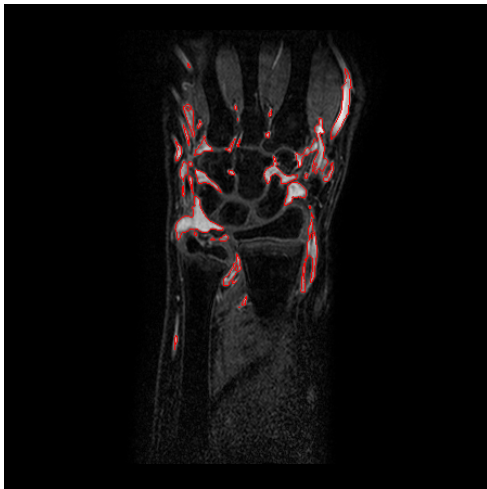
Results for classifiers trained and tested on one observer. Different normalizations.

	-	Scaling	Ranking
	Classification Error		
ITAO	9.8%	8.5%	8.7%
ITEC	9.3%	7.7%	8.2%
ITMB03	7.8%	7.0%	7.7%
ITMB29	8.7%	8.0%	8.7%
mean	8.9%	7.8%	8.3%
σ	0.86%	0.63%	0.48%
	Volume Error		
ITAO	1.0%	-53.6%	-38.4%
ITEC	-64.6%	-9.7%	-49.3%
ITMB03	-71.4%	-47.2%	-27.8%
ITMB29	-6.4%	-43.1%	-34.8%
mean	-35.4%	-38.4%	-37.6%
σ	37.9%	19.6%	9.0%

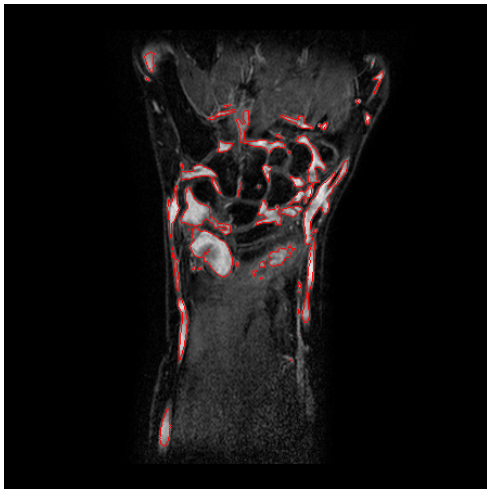
Results on Unlabeled Data

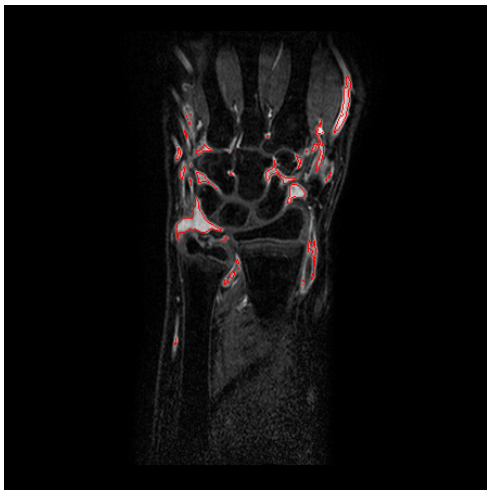


Results on Unlabeled Data

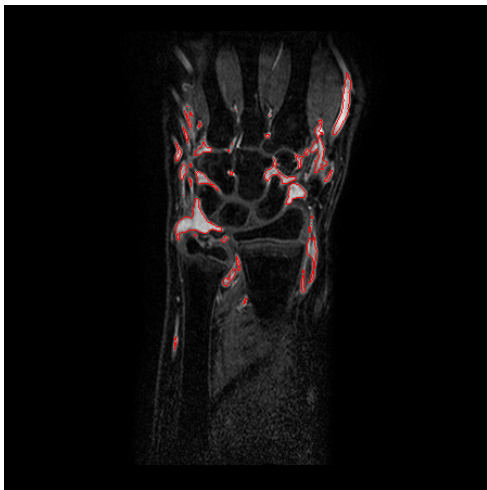


Results on Unlabeled Data

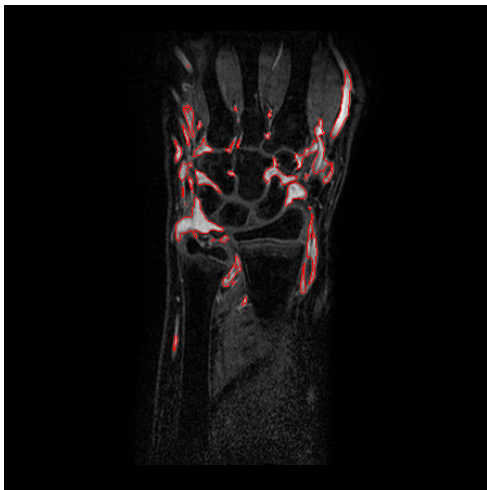




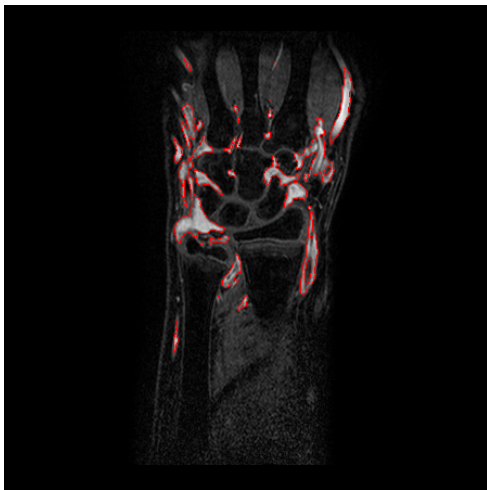
$$b = b_0 - 0.3$$



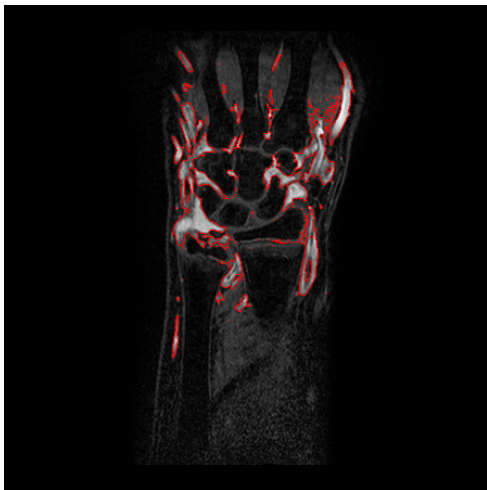
$$b = b_0$$



$$b = b_0 + 0.3$$



$$b = b_0 + 0.6$$



$$b = b_0 + 0.9$$

Other enhanced structures (blood vessels, sinew) are selected.
They have to be removed

Mixed approach:

- some structures (e.g. vessels) might be detected based on their shape, and can be removed automatically;
- however, there might be structures more difficult to detect, which will have to be removed manually.